

1 **Reliability of Continuous Shear Wave Elastography in the Pathological Patellar Tendon**

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24 **Abstract:**

25 Objectives: Patellar tendon injuries occur via various mechanisms such as overuse, or due to
26 surgical graft harvest for anterior cruciate ligament reconstruction (ACLR). Quantified patellar
27 tendon stiffness after injury may help guide clinical care. Continuous shear wave elastography
28 (cSWE) allows for the assessment of viscosity and shear modulus in tendons. The reliability of the
29 measure, however, has not been established in the patellar tendon. The purpose of this study was
30 to investigate the inter-rater reliability, intra-rater reliability, and between day stability of cSWE
31 in both healthy and pathological patellar tendons.

32 Methods: Participants with patellar tendinopathy (n = 13), history of ACLR using bone-patellar
33 tendon-bone autograft (n = 9), and with no history of patellar tendon injury (n = 13) were recruited.
34 cSWE was performed 4 times by multiple raters over 2 days. Intra-class correlations (ICC) and
35 minimum detectable change (MDC_{95%}) were calculated.

36 Results: Good to excellent between day stability were found for viscosity (ICC = 0.905, MDC_{95%}
37 = 8.3Pa*s) and shear modulus (ICC = 0.805, MDC_{95%} = 27.4kPa). The inter-rater reliability
38 measures, however, were not as reliable (ICC = 0.591 and 0.532).

39 Conclusions: cSWE is a reliable assessment tool for quantifying patellar tendon viscoelastic
40 properties over time. It is recommended, however, that a single rater performs the measure as the
41 inter-rater reliability was less than ideal.

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43 **Keywords:** viscoelastic properties, patellar tendon, continuous shear wave elastography, anterior
44 cruciate ligament, tendinopathy, bone-patellar tendon-bone graft

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46 **Introduction:**

47 Patellar tendon injuries are common amongst athletes of all levels (recreational to professional)
48 and age groups, and may become a significant burden for those who suffer such injuries ^{1,2}. One
49 of the themes observed across pathological tendons, regardless of the source of injury, are
50 morphological alterations (e.g., tendon thickening, larger cross-sectional areas, or hypoechoic
51 regions identified on sonographic evaluations) to the tendon ³. Tendon structure is associated with
52 function and outcomes after injury, and may be readily assessed in a clinical setting ⁴⁻⁸. Evaluating
53 the structural changes in the injured patellar tendon may assist in identifying the underlying
54 pathophysiology as well as guide clinical care after injury.

55 Patellar tendinopathy is an overuse injury of the patellar tendon typically associated with activities
56 involving plyometrics ^{9,10}. Prevalence of patellar tendinopathy has been reported as high as 45%
57 in higher level jumping athletes ². Tendon injury may also be of iatrogenic nature after procedures
58 such as graft harvest of the bone-patellar tendon-bone (BPTB) autograft during anterior cruciate
59 ligament reconstruction (ACLR) ¹¹. The BPTB autograft, harvested from the central third of the
60 patellar tendon, is frequently used due to the low re-rupture rates reported in active young adults
61 compared to alternative graft types ^{12,13}. The use of a BPTB autograft, however, comes with
62 secondary impairments specific to the graft harvest site. Prolonged quadriceps weakness ^{14,15}, a
63 metric associated with successful outcomes after ACL surgery has been identified ¹⁶, likely
64 because of the additional trauma to the extensor mechanism. Anterior knee pain also persists after
65 using BPTB autografts ^{17,18} and rates of post-traumatic knee osteoarthritis may also be elevated
66 ^{19,20}. In both populations described above, understanding the injured tendon's structure may assist
67 in improving our knowledge on the underlying pathophysiology and assist in guiding post-injury
68 or post-operative care to optimize outcomes.

69 Morphological (e.g., thickness and cross-sectional area) changes to injured tendons assessed using
70 B-mode ultrasound and magnetic resonance imaging have been observed with time after surgery
71 and rehabilitation in patients after tendon pathology^{5,21-24}. It is also known, however, that
72 improvements in symptoms and function can happen without morphological changes²⁵. The
73 variability and mismatch in morphological and symptom presentation along the course of
74 rehabilitation, may in part be due to changes in the underlying viscoelastic properties (i.e.,
75 stiffness) of the tendon which may not be captured with traditional imaging modalities^{7,26-29}.
76 Assessing viscoelastic properties of the patellar tendon may provide additional knowledge beyond
77 measuring morphology alone when identifying pathological tendons and tracking changes over
78 time.

79 Methods using shear wave elastography to quantify stiffness in the musculoskeletal system have
80 become increasing popular in recent years due to the low risk and non-invasive approach to
81 quantify and track tissue mechanical properties²⁹⁻³². Continuous shear wave elastography (cSWE)
82 is an ultrasound-based method to evaluate tendon viscoelastic properties as biomarkers for injury
83 and recovery³³. cSWE involves measuring wave speeds of shear waves transduced through a
84 tendon using an external actuator³⁴⁻³⁶ to calculate two coefficients of interest in viscoelastic
85 materials, shear modulus (kPa) and viscosity (Pa-s). The method has been validated in the Achilles
86 tendon and demonstrated fair to excellent intra-rater reliability³⁷. The reliability of cSWE in the
87 patellar tendon, tendons with pathology (tendinopathy or graft harvest), or the inter-rater reliability
88 of cSWE, however, has not been established. The purpose of this study was to investigate the inter-
89 rater reliability, intra-rater reliability, and between day stability of cSWE in both healthy and
90 pathological patellar tendons.

91 **Materials and Methods:**

92 **Participants:**

93 An a priori power analysis was completed using methods based on a lower acceptable limit ³⁸.
94 Fourteen participants were required with two raters, a desired reliability of ICC = 0.9, lower
95 acceptable limit of ICC = 0.6, $\beta = 0.8$, and $\alpha = 0.05$. Thirteen participants with patellar
96 tendinopathy (PT), 9 participants with a history of bone-patellar tendon-bone graft harvest for
97 ACLR (BPTB), and 13 participants with no current or history of patellar tendon injury (Healthy)
98 were recruited for this study (**Table 1**). Participants in the tendinopathy group all had symptomatic
99 patellar tendinopathy confirmed by a licensed physical therapist (A.S.) at the time of data
100 collection, and the participants in the BPTB group were included in the study regardless of patellar
101 tendon symptoms at the time of testing. This study was approved by the institutional review board
102 at the University of Delaware and participants provided written informed consent.

103 **Study Design:**

104 cSWE was performed by 4 different raters (**Table 2**) of varying levels of experience performing
105 cSWE. Rater A, the most experienced rater, and rater B, the rater with the least amount of
106 experience who received 2 hours of training for familiarization of the methods performed all data
107 collections for the patellar tendinopathy group. Rater C and D performed all data collections for
108 the healthy and BPTB group. Rater A and C were assigned as the primary rater to compare for
109 intra-rater reliability and between day stability, while measurements from rater B and D were
110 assigned as secondary raters used to calculate inter-rater reliability.

111 cSWE was performed in two sessions approximately 24 hours apart (**Figure 1**). Participants were
112 encouraged to avoid any strenuous exercise 24 hours prior to each test session. On day 1, the
113 primary raters (A and C) performed 1 round of cSWE. On day 2, the primary raters performed 2

114 rounds of cSWE followed by the secondary raters (B and D) performing 1 round of cSWE.
115 Between trials on day 2, participants were asked to stand up and walk a single loop around the
116 room to reset positioning for the test, and all markings indicated on the participants' knees were
117 removed using alcohol wipes (**Figure II**). The patellar tendon of interest (right vs. left) was
118 determined using the surgical knee for the BPTB group, the symptomatic side (or the most
119 symptomatic side if the participant experienced bilateral symptoms) for the tendinopathy group,
120 and a random number generator was used to choose the side of interest in the healthy control group.

121 **Continuous Shear Wave Elastography (cSWE):**

122 Participants were positioned in an upright chair with both hips and knees position at 90 degrees of
123 flexion. Both feet were strapped in a custom setup made of controlled ankle motion boots for
124 stabilization and to limit muscle contractions and movement artifact (**Figure II**). The region of
125 interest over the patellar tendon was marked using a marker after inspecting the patellar tendon
126 using ultrasound imaging (**Figure II**). For the BPTB group, the region of interest was over the
127 central third where the graft was harvested. For the tendinopathy group, the measurement was
128 taken 1 cm distal to the inferior pole of the patella. For the healthy control group, the patellar
129 tendon was trisected vertically, and the central third of the patellar tendon was measured. An
130 ultrasound scanner (Ultrasonix, Vancouver, BC, Canada) with a L14-5/38 probe was used to
131 capture raw radiofrequency data over the region of interest (6438 frames per second), while an
132 external actuator (Minshaker Type 4810, Bruel and Kjaer, Norcross, GA, USA) was placed over
133 the quadriceps tendon just superior to the patella to produce shear waves. The ultrasound probe
134 was placed parallel with the longitudinal axis of the region of interest and stabilized using a 3-
135 prong clamp (**Figure II**).

136 Shear waves at 11 fixed frequencies (322, 339, 358, 379, 402, 429, 460, 495, 536, 585, and 643Hz)
137 were produced at the quadriceps tendon while the raw radiofrequency data were collected
138 simultaneously (**Figure III**). All 11 frequencies were produced and captured independently while
139 the knee and ultrasound probe were secured in the same position. Ultrasound data were collected
140 for 10 ms for each of the frequencies. Three successful trials were collected during each test while
141 the ultrasound probe was removed and repositioned between each trial to confirm proper contact
142 and placement over the region of interest. A custom MATLAB script was used to calculate static
143 shear modulus and viscosity using data from all 11 frequencies using the Voigt model for
144 viscoelasticity which has been detailed in previous work³³. The average shear modulus and
145 viscosity of the three trials collected were calculated and reported.

146 **Statistics:**

147 Three separate reliability measures for both shear modulus and viscosity were calculated using
148 intra-class correlations (ICC). *Between-day intra-rater stability (Trial 1 vs. Trial 2)* and *within-*
149 *day intra-rater reliability (Trial 2 vs. Trial 3)* were calculated using a mean-rating, absolute
150 agreement, two-way mixed effects model. *Within-day inter-rater reliability (Trial 2 vs. Trial 4)*
151 was calculated using a mean-rating, absolute agreement, one-way random effects model³⁹. ICCs
152 were calculated for the complete sample combining data from both healthy and pathological
153 patellar tendons (n=35), and separately using the data from only the pathological patellar tendons
154 (n=22) for comparison. The standard error of the measurement (SEM) and individual minimum
155 detectable change (MDC_{95%}) at the 95% confidence interval were calculated using ICC values
156 obtained from the two cohorts. Group MDC_{95%} were also calculated within our sample (Group
157 MDC_{95%} = Individual MDC_{95%} / \sqrt{n}) for comparisons between the 3 groups in our study.

158 As a secondary purpose, one-way analysis of variance ($\alpha=0.05$) was used to compare shear
159 modulus and viscosity among the three groups (PT, BPTB, Healthy). The assumptions for
160 normality and homogeneity were met. Pair-wise comparisons were performed for significant main
161 effects of group. All statistics were performed using R⁴⁰.

162 **Results:**

163 For the complete sample, excellent between day stability was observed for viscosity (ICC = 0.905),
164 and good between day stability was observed for shear modulus (ICC = 0.805). Good within-day
165 intra-rater reliability was observed for both viscosity and shear modulus (ICC = 0.839 and 0.751).
166 Moderate inter-rater reliability was observed for both viscosity and shear modulus (ICC = 0.591
167 and 0.532). The individual MDC_{95%} of the measures were identified to be 8.3Pa*s for viscosity,
168 and 27.4kPa for shear modulus (**Table 3**). ICC outcomes using only the pathological patellar
169 tendons (**Table 4**) identified similar reliability measures compared to the complete sample
170 including healthy patellar tendons.

171 Main effects of group were observed for both shear modulus ($F(2, 32) = 4.43, p = 0.020, \eta_p^2 =$
172 0.217) and viscosity ($F(2, 32) = 4.33, p = 0.022, \eta_p^2 = 0.213$) (**Table 5**). Pairwise comparisons
173 identified for viscosity, that the PT group presented with higher viscosity compared to both the
174 BPTB ($p = 0.013$) and Healthy ($p = 0.025$) groups. No differences were found between the BPTB
175 and Healthy groups ($p = 0.612$). For shear modulus, the PT group presented with higher shear
176 modulus compared to the BPTB group ($p = 0.007$) and the difference between the Healthy group
177 trended towards significance ($p = 0.052$). No differences were found between the BPTB and
178 Healthy groups ($p = 0.308$).

179 **Discussion:**

180 The purpose of this study was to investigate the inter-rater reliability, intra-rater reliability, and
181 between day stability of cSWE in both healthy and pathological patellar tendons. Our study
182 findings indicate good to excellent reliability for both viscosity and shear modulus measures
183 obtained via cSWE when repeat measures were collected by a single rater. The inter-rater
184 reliability of the measure, however, only demonstrated moderate reliability, emphasizing the
185 importance of a single rater performing cSWE when used in any study design.

186 The good to excellent reliability found in this study is comparable to what has been reported in the
187 Achilles tendon³⁷. Additionally, this study supports the reliability of using cSWE not only in
188 healthy tendons but also in pathological tendons as comparable ICCs were observed (**Table 3 and**
189 **4**). The comparison between groups identified that the PT group may present with higher shear
190 modulus and viscosity compared to the 2 other groups in this study, possibly indicating the
191 underlying source of pathology and symptoms (**Table 5**). No differences were found between the
192 BPTB and Healthy groups, and this finding is likely due to the sampling strategy for the BPTB
193 group which was not optimized for detecting group differences (**Table 1**). Symptoms were not a
194 part of inclusion criteria for the BPTB group as the primary objective of the study was to establish
195 reliability, and participants from a large range of time from surgery were included to strengthen
196 external validity for the reliability measure in this population. A more homogeneous sample in the
197 BPTB group such as those with symptomatic patellar tendons or those acutely after ACLR is
198 necessary to establish clinical meaning of the mechanical properties measured using cSWE. While
199 a larger sample size is needed to further establish group differences in tendon viscoelastic
200 properties, our data from a limited sample provides promising insight for future use of cSWE.
201 cSWE can be used as a reliable tool in future studies investigating long term changes in the patellar

202 tendon over the course of treatment for patellar tendinopathy or recovery after BPTB autograft
203 harvest for ACLR.

204 The relatively low inter-rater reliability compared to intra-rater reliability was an unexpected
205 finding. While no definitive conclusions can be drawn from our data, we have identified potential
206 sources of error that may explain this finding. The initial scanning of the patellar tendon to identify
207 region of interest is the first likely reason. The ultrasound probe is only able to image a 1mm width
208 region (credit card thickness), and it is likely the region selected varied between raters. The
209 variability in alignment of the probe with the tendon fibers may also affect values recorded for
210 shear wave speed due to tendon anisotropy. We do, however, report the average of 3 repositioned
211 trials to limit this error, and the slight variation within the region captured is intended to capture a
212 more representative image of each region. To improve inter-rater reliability of cSWE, an average
213 of more than 3 trials may be necessary. Other sources of error may be from the amount of pressure
214 applied at the ultrasound probe on the patellar tendon or the external actuator at the quadriceps
215 tendon. Especially at the quadriceps tendon, since the rater manually held the actuator, there may
216 have been variability in the pressure or steadiness of the hand holding the actuator resulting in
217 slightly different shear waves transferred through the tendon. Future studies may investigate the
218 influence of taking the average of more trials or controlling for ultrasound probe and actuator
219 pressure and steadiness, to see if inter-rater reliability can be improved. Lastly, exercise between
220 the 2 days of study visits were not tightly controlled due to ethical reasons, since participation in
221 rehabilitation was a priority for the participants who were currently undergoing treatment. The
222 participants' activity level between study days may have influenced reliability in tendon
223 mechanical properties.

224 Continuous shear wave elastography is a reliable assessment tool of the viscoelastic properties in
225 the patellar tendon with pathology. It is recommended, however, that a single rater performs all
226 tests, as the inter-rater reliability of the measure was found to be less reliable in this study.

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233

234 **Conflict of interest:**

235 The authors of this manuscript have no conflicts of interest to disclose.

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368

369

370 **Table 1:**

371 Participant demographics by group. PT = Patellar tendinopathy, BPTB = Bone-Patellar Tendon-

372 Bone graft, Healthy = Healthy control, All = all participants combined.

Group	Sex (women:men)	Age (years)	Height (meters)	Weight (kilograms)	Symptom Duration (months [range])	Time from Surgery (months [range])
PT	4:9	31.2±9.4	1.79±0.10	80.8±17.0	33.8 [1.0 - 93.1]	-
BPTB	5:4	22.9±5.6	1.73±0.13	72.7±19.9	-	28.2 [1.6 - 91.7]
Healthy	6:7	26.2±2.4	1.76±0.09	76.0±8.4	-	-
All	15:20	27.2±7.2	1.76±0.11	76.9±15.2	-	-

373

374

375 **Table 2:**

376 Clinical and ultrasound experience of each rater.

Raters	Clinical Credentials	Years since licensure	Experience with ultrasound imaging	Experience with cSWE
A	Physical Therapist	4 years	4 years	4 years
B	None	-	No experience	2 hours
C	Physical Therapist	1 year	2 years	1 year
D	Physical Therapist	12 years	2 years	1 year

377

378

379 **Table 3:**

380 Reliability and minimum detectable change of the complete sample (n=35). ICC = intra-class
381 correlation, 95%CI = 95% confidence interval, SD = standard deviation, SEM = standard error of
382 measure, MDC_{95%} = minimum detectable change, kPa = kilopascals, Pa*s = Pascal-seconds.
383 Highlighted in yellow = ICC and MDC relevant for assessing tendon changes over time.

Shear Modulus (kPa)	ICC	95%CI		Pooled Mean	Pooled SD	SEM	MDC _{95%}
	Average Measures	Lower	Upper				Individual
Stability	0.805	0.657	0.890	68.2	22.4	9.9	27.4
Intra-rater	0.751	0.562	0.859	65.8	22.8	11.4	31.6
Inter-rater	0.532	0.176	0.735	67.0	21.1	14.4	40.0
Viscosity (Pa*s)							
Stability	0.905	0.833	0.946	25.3	9.7	3.0	8.3
Intra-rater	0.839	0.705	0.910	24.1	9.7	3.9	10.8
Inter-rater	0.591	0.279	0.769	25.5	9.1	5.8	16.1

384

385 Footnote:

386 Excellent reliability: ICC > 0.9, Good reliability: 0.75 < ICC < 0.9, Moderate reliability: 0.5 < ICC
387 < 0.75, Poor reliability: ICC < 0.5³⁹

388

389 **Table 4:**

390 Reliability and minimum detectable change of the pathological tendons only (i.e., PT and BPTB
391 groups) (n=22). ICC = intra-class correlation, 95%CI = 95% confidence interval, SD = standard
392 deviation, SEM = standard error of measure, MDC_{95%} = minimum detectable change, kPa =
393 kilopascals, Pa*s = Pascal-seconds. Highlighted in yellow = ICC and MDC relevant for assessing
394 tendon changes over time.

Shear Modulus (kPa)	ICC	95%CI		Pooled Mean	Pooled SD	SEM	MDC _{95%}
	Average Measures	Lower	Upper				Individual
Stability	0.817	0.624	0.912	68.6	22.8	9.8	27.1
Intra-rater	0.813	0.616	0.909	68.4	22.9	9.9	27.4
Inter-rater	0.424	-0.185	0.722	65.8	20.0	15.2	42.0
Viscosity (Pa*s)							
Stability	0.933	0.863	0.968	27.3	10.4	2.7	7.4
Intra-rater	0.880	0.753	0.942	26.0	10.4	3.6	10.0
Inter-rater	0.644	0.266	0.828	26.3	9.8	5.9	16.3

395

396 Footnote:

397 Excellent reliability: ICC > 0.9, Good reliability: 0.75 < ICC < 0.9, Moderate reliability: 0.5 < ICC
398 < 0.75, Poor reliability: ICC < 0.5 ³⁹

399

400 **Table 5:**

401 Shear modulus and Viscosity by group. PT = Patellar tendinopathy, BPTB = Bone-Patellar

402 Tendon-Bone graft, Healthy = Healthy control, kPa = kilopascals, Pa*s = Pascal-seconds.

Group	Shear modulus (kPa)	Viscosity (Pa*s)
PT	80.3±16.4	31.3±10.5
BPTB	57.1±16.3	20.1±7.9
Healthy	65.5±22.1	22.9±8.6

403

404

405 **Figure Legends**

406 **Figure 1:**

407 Title: Reliability measures of interest

408 Description: Inter- and intra- rater reliability was assessed within the same day and between day
409 intra-rater stability was assessed 24 hours apart.

410 **Figure 2:**

411 Title: cSWE set up

412 Description: Participants were seated with their hips and knees at 90 degrees of flexion with their
413 lower leg stabilized in a custom boot (right). The ultrasound probe was placed on a custom clamp
414 after the region of interest was determined, and the external actuator was placed on the quadriceps
415 tendon above the knee held by the rater (left).

416 **Figure 3:**

417 Title: Shear wave propagation through the patellar tendon

418 Description: Shear wave speeds measured within the region of interest for the 11 frequencies were
419 then used to calculate viscosity and shear modulus using the Voigt model³³. The images reflect an
420 example trial from one of the healthy patellar tendons at the 322Hz frequency.